

1 **Encapsulation of food waste compounds in soy phosphatidylcholine liposomes: effect of**  
2 **freeze-drying, storage stability and functional aptitude**

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7  
8 Abstract

9 Liposomes made from soy phosphatidylcholine entrapping food waste compounds (collagen  
10 hydrolysate, L-HC; pomegranate peel extract, L-PG; and shrimp lipid extract, L-SL) were freeze-  
11 dried and stored for seven months. The freeze-drying process increased the particle size and  
12 decreased water solubility. The freeze-dried L-HC and L-PG preparations presented large  
13 multivesicular vesicles with spherical and unilamellar morphology. Large multilamellar vesicles  
14 were observed in L-SL, coinciding with greater structural changes in the membrane bilayer and  
15 increased thermal stability, as observed by ATR-FTIR and DSC. Dynamic oscillatory rheology  
16 revealed a slight hardening in the dried liposomes, induced by storage time. A sharp rigidifying  
17 effect in the temperature range from 40 to 90 °C was observed in L-SL. The loading with  
18 antioxidant compounds prevented freeze-drying-induced lipid oxidation. The storage stability  
19 of freeze-dried liposomes and their technological aptitude as a food ingredient varied  
20 depending on the chemical nature of the entrapped compounds.

21  
22 Keywords: food; liposomes; soy phosphatidylcholine; lipid oxidation; freeze-drying; storage  
23 stability.

## 25 **1. Introduction**

26 Nowadays there is growing interest in the use of liposomes in the food industry in a variety of  
27 applications (Mozafari et al., 2008). Liposomes carrying bioactive compounds could be  
28 incorporated in functional foods for enrichment with healthy components or diseases  
29 prevention (Singh, 2016). Soy phosphatidylcholine-based liposomes have been used for  
30 encapsulating omega-3, omega-6, and vitamins E and C to fortify chocolate milk (Marsanasco  
31 et al., 2016) or orange juice (Marsanasco et al., 2015). The use of natural soybean lecithin for  
32 liposomal encapsulation in food applications provides nutritional value owing to its high  
33 essential polyunsaturated fatty acid profile with a beneficial role in lipid metabolism (Ramdath  
34 et al., 2017), and it does not raise any food legislation concerns (Laye et al., 2008). However,  
35 the predominantly highly unsaturated nature of soy lecithin could make this material very  
36 susceptible to lipid oxidation (Wang and Wang, 2008).

37 Liposomes are amphipathic spherical colloidal vesicles composed of one or more phospholipid  
38 bilayers around an aqueous core. This feature enables them to entrap and protect both  
39 hydrophilic and lipophilic bioactive materials, and to act as target delivery carriers in the  
40 organism (Mozafari et al., 2008). There is extensive recently published information on  
41 phosphatidylcholine liposomes loaded with a great variety of natural compounds with  
42 antioxidant properties, such as gelatin or collagen hydrolysates (Ramezanzade et al., 2017;  
43 Mosquera et al., 2014), polyphenolic compounds (Popova and Hinch, 2016; Lopes de  
44 Azambuja et al., 2015), or strong lipophilic compounds such as carotenoids (Du et al., 2015),  
45 tocopherol (Neunert et al., 2015) or essential polyunsaturated fatty acids (Semenova et al.,  
46 2016). However, differences in liposome composition and production procedure make it  
47 difficult to compare the physico-chemical properties of the resulting loaded vesicles.

48 Liposomes are normally presented in the form of aqueous liposomal suspensions, which could  
49 lose stability causing vesicle fusion or aggregation, leakage of the entrapped compounds and

50 sedimentation (Sharma and Sharma, 1997). Lyophilization is an alternative process for  
51 increasing the shelf life of liposomes, maintaining their stability by preserving them in a dry  
52 state (Stark et al., 2010). Drying liposomes is also a technological way of including vesicles in  
53 restructured fish products without negatively affecting their water content (Marín et al., 2018).  
54 However, freeze-drying may damage lipid bilayers by ice crystal formation during freezing,  
55 vesicle fusion/aggregation following dehydration and changes in phase transition during  
56 rehydration (Chen et al., 2010). Cryoprotectants, such as carbohydrates or polyalcohols, have  
57 been proposed to prevent freeze-drying-induced vesicle damage (Stark et al., 2010).

58 The aim of this work was to study the effect of freeze-drying and long-term storage on  
59 physico-chemical, structural, rheological and oxidative properties of glycerol-added liposomes  
60 entrapping various heat-sensitive food waste compounds with high added value, which could  
61 be used as functional food ingredients.

62

## 63 **2. Materials and methods**

### 64 **2.1. Extraction of food waste compounds**

65 Alcalase acid-soluble collagen hydrolysate (HC) was obtained from frozen squid (*Dosidicus*  
66 *gigas*) tunics following the procedure described in a previous work (Marín et al., 2018). The HC  
67 was spray-dried and stored at -20 °C until use. The HC hydrolysate was mostly composed of <  
68 1.3 kDa peptide fractions (89 %), with major constituent amino acid residues of glycine,  
69 glutamic acid, alanine and aspartic acid (56 %), and total hydrophobic amino acids accounting  
70 for 28 % (Marín et al., 2018).

71 Pomegranate (*Punica granatum*) peel and albedo were dried in an oven at 50 °C overnight and  
72 grounded to obtain a fine powder, which was suspended in ethanol/water (70/30) at 1:20  
73 (w/v) ratio and stirred at 40 °C for 4h. The mixture was left to stand at 21 °C overnight and

74 centrifuged at 12000g (at 4 °C for 15 min). The supernatant was filtered through Whatman  
75 No.1 paper. The obtained extract (PG) was rotary-evaporated at 40 °C and stored at –20 °C  
76 until use. The PG extract was mainly composed of ellagitannins ( $\beta$ -punicalagin, ellagic acid, and  
77  $\alpha$ -punicalagin), being rutin and epigallocatechin also identified. The total phenolic content in  
78 PG was 166 mg gallic acid eq./g dry extract (Marín et al., 2018).

79

80 The ethyl acetate-soluble lipid extract from shrimp (*L. vannamei*) waste (SL) was prepared and  
81 characterized in a previous work (Gómez-Estaca et al., 2017). The SL extract was composed of  
82  $\approx$ 80 % fatty acids,  $\approx$ 13 %  $\alpha$ -tocopherol, 6.5 % cholesterol and 0.7 % astaxanthin (free and  
83 esterified). The PUFA proportion was 44 %. The SL was rotary-evaporated at 60 °C and stored  
84 at –20 °C until use.

85

## 86 **2.2. Preparation of liposomes**

87 Partially purified phosphatidylcholine (PC) was obtained by dissolving soybean lecithin in ethyl  
88 acetate (1:5, w/v) and subsequently performing five washes with acetone (Taladrid et al.,  
89 2017). The PC powder was stored at –20 °C until use.

90 Liposomes L-HC, L-PG and L-SL were produced according to Marín et al. (2018). Each extract  
91 (0.8 g) was dispersed in 80 mL of 0.2 M phosphate buffer (pH 7). Then PC (20 g) was added and  
92 the dispersions were kept in a water bath at 80 °C for 1 h. Phosphate buffer (68 mL) and  
93 glycerol (12 mL) were added, and the mixtures were kept at 80 °C for 1 h. The volume of the  
94 suspension was completed with 240 mL of phosphate buffer. The samples were vortexed at 60  
95 °C and sonicated in an ultrasonic cell disrupter (Model Q700, Qsonica sonicators, Newton, CT,  
96 USA). The hydrodynamic particle stability of the newly prepared liposomal dispersions was  
97 measured during two weeks at 4 °C. The freeze-drying process was performed by placing 50mL

98 of newly prepared liposomal dispersion in plastic cups of 100mL with perforated caps, which  
99 were frozen at -80 °C for 24h. Lyophilisation took place in a VirTis Freeze Drying Equipment  
100 (VirTis mod.6K TEL-85, coupled to TRIVAC-E2 pump) operating at a vacuum level of 0.13 mbar,  
101 with the collector starting at a temperature of -45 °C up to -80°C after 48h. All dried liposomes  
102 presented a pasty-like consistency rather than a fine powder appearance. The freeze-dried  
103 liposomes (liposomal pastes) were stored in darkness at -20 °C for seven months, in order to  
104 check their long-term storage stability.

### 105 **2.3. Size, polydispersity and zeta potential**

106 Particle size (z-average in intensity), polydispersity index (PDI) and zeta potential of fresh and  
107 rehydrated liposomes were measured using a Zetasizer Nano ZS (Malvern Instruments Ltd,  
108 Worcestershire, UK) in triplicate at 25 °C (Alemán et al., 2016). Freeze-dried liposomes were  
109 previously rehydrated by suspending in distilled water (77 mg/mL) at 20 °C for 30 min under  
110 magnetic stirring.

### 111 **2.4. Entrapment efficiency**

112 The entrapment efficiency (EE) was determined following the procedure of Marín et al. (2018),  
113 and calculated by the equation:

$$114 \quad \% EE = \text{encapsulated extract} / \text{total extract} * 100.$$

115 The encapsulated extract was calculated by difference between the total extract and the non-  
116 encapsulated extract. The non-encapsulated extract was quantified by: protein content with a  
117 LECO FP-2000 nitrogen/protein analyser for HC; phenolic content by the Folin-Ciocalteu  
118 method for PG; and astaxanthin content by spectrophotometric absorbance measurement at  
119 470 nm for SL.

120

121 **2.5. Moisture content and water solubility**

122 Moisture was determined according to method 950.46 (A.O.A.C., 2005). Water solubility was  
123 determined after dilution in distilled water (1% w/v) at 20 °C for 150 min under magnetic  
124 stirring and centrifugation at 5000 g at 4 °C for 5 min. The supernatant was dried at 105 °C and  
125 the water solubility, expressed as a percentage, was calculated by weight difference with  
126 respect to the initial sample weight.

127

128 **2.6. Cryo-transmission electron microscopy (cryo-TEM)**

129 Cryo-TEM images of freeze-dried liposomes were obtained at –180 °C, using a JEOL JEM-1230  
130 transmission electron microscope operating at 100 kV with a nominal magnification of 30K, as  
131 described previously (Taladrid et al., 2017).

132

133 **2.7. Colour**

134 The colour parameters, L\* (lightness), a\* (redness) and b\* (yellowness) of freeze-dried  
135 liposomes, were measured using a Konica Minolta CM-3500d colorimeter (Konica Minolta,  
136 Madrid, Spain), with D65 illuminant and D10 standard observer. Hue angle and chroma values  
137 were calculated from L\* a\* b\* values. Results were the average of 10 replicates.

138

139 **2.8. Differential Scanning Calorimetry (DSC)**

140 DSC analysis was performed using a model TA-Q1000 differential scanning calorimeter (DSC)  
141 (TA Instruments, New Castle, DE, USA) (Taladrid et al., 2017). All samples (≈10–12 mg) were  
142 scanned at a heating rate of 10 °C/min from –35 °C to 90 °C, under dry nitrogen purge (50  
143 mL/min). Endothermic peak temperatures ( $T_{peak}$ , °C) and enthalpies of conformational changes  
144 ( $\Delta H$ , J/g) were determined at least in triplicate.

145

## 146 **2.9. Attenuated Total Reflectance Infrared spectroscopy (ATR-FTIR)**

147 Infrared spectra of freeze-dried liposomes were recorded between 4000 and 650  $\text{cm}^{-1}$  using a  
148 Perkin Elmer Spectrum 400 Infrared Spectrometer (Perkin Elmer Inc., Waltham, MA, USA)  
149 equipped with an ATR prism crystal accessory as described previously (Taladrid et al., 2017).

150

## 151 **2.10. Dynamic oscillatory rheology**

152 Viscoelastic properties ( $G'$ ,  $G''$ ,  $\delta$ ) of freeze-dried liposomes were determined in a Bohlin  
153 rheometer (Bohlin Instruments Ltd., model CVO-100, Worcestershire, UK), using a cone-plate  
154 geometry (cone angle 4°, gap 0.15 mm). A dynamic frequency sweep was performed by  
155 applying oscillation amplitude at 5% strain over the frequency range 0.1–10 Hz at 10 °C. The  
156 mechanical spectra with the elastic modulus ( $G'$ ; Pa) and viscous modulus ( $G''$ ; Pa) were  
157 plotted as functions of frequency. To characterize the frequency dependence of  $G'$  over the  
158 limited frequency range, the power law was used:

159

$$G' = G_0' \omega^{n'}$$

160 where  $G_0'$  is the energy stored and recovered per cycle of sinusoidal shear deformation at a  
161 frequency of 1 Hz,  $\omega$  is the frequency and  $n'$  is the power law exponent, which should exhibit  
162 an ideal elastic behaviour near zero. A temperature sweep test was performed by heating from  
163 20 to 90 °C at 1 °C/min and frequency of 1 Hz. Values of  $G'$  and  $G''$  were plotted as functions of  
164 temperature. At least two determinations were performed for each sample. The experimental  
165 error was lower than 6% in all cases.

166

## 167 **2.11. Lipid oxidation**

168 Lipid oxidation was measured by the thiobarbituric acid reactive substances (TBARS) method.  
169 Liposomes were mixed with 7.5% trichloroacetic acid solution (1:3 w/v) and centrifuged at  
170 5100 g for 5 min at 4 °C. Then 0.02 M thiobarbituric acid was added to the supernatant (2:1  
171 v/v) and kept at 20 °C for 15 hours in darkness. Absorbance was measured at 532 nm. Results  
172 were expressed as µg of malondialdehyde (MDA) equivalent per kg of sample, based on a  
173 1,1,3,3-tetraethoxypropane (TEP) standard curve. Samples were analysed at least in triplicate.

174

## 175 **2.12. Statistical analyses**

176 Analysis of variance was performed using the SPSS® computer program (IBM SPSS Statistics 22  
177 Software, Inc., Chicago, IL, USA). Differences among samples were established using the Tukey  
178 test, with a significance level set at  $p \leq 0.05$ .

179

## 180 **3. Results and discussion**

### 181 **3.1. Particle characterization**

182 The three freshly loaded liposomes did not differ ( $p > 0.05$ ) in particle size, polydispersity index  
183 and zeta potential (Table 1). The empty liposomes (L-E) presented lower ( $p \leq 0.05$ ) z-average  
184 and zeta potential than the loaded liposomes. The PDI, which reflects particle size distribution,  
185 oscillated between 0.24 and 0.26; the PDI is considered a good index when it is below 0.3. The  
186 strong electronegative zeta potential values were indicative of the high stability of all the  
187 liposomal suspensions (Müller et al., 2001). The loading with HC, PG or SL contributed slightly  
188 to an increase in the surface membrane charge, providing increased stability to the respective  
189 liposomal suspensions.



190 Fresh liposomes stored at 4 °C for 2 weeks showed no significant changes in size and PDI, while  
191 the zeta potential experienced only a very slight decrease ( $p \leq 0.05$ ) in L-HC and L-SL at the end  
192 of the second week of storage (Table 1). These results confirmed the high stability of the fresh  
193 liposomal suspensions during short-term storage.

194 The freeze-drying process caused increases ( $p \leq 0.05$ ) in the liposome z-average and zeta  
195 potential (Table 1). The changes in PDI were more accentuated in L-SL, which changed from  
196 0.246 to 0.408. An increase in size and polydispersity when a small liposome is freeze-dried has  
197 been reported previously and attributed to fusion or aggregation phenomena during water  
198 removal (Chen et al., 2010) and to swelling of the bilayer upon rehydration (Stark et al., 2010).

199 To check the storage stability of the freeze-dried liposomes, their particle properties after  
200 rehydration were characterized at 0, 3 and 7 months (Table 1). Immediately after freeze-  
201 drying, L-SL had the largest size and polydispersity. The zeta potential was similar in all  
202 formulations and showed a slight tendency to decrease ( $p \leq 0.05$ ) with time. The liposomes with  
203 the entrapped compounds showed a decrease ( $p \leq 0.05$ ) in z-average at month 3, while the  
204 empty liposome showed a more gradual size reduction from months 0 to 7. The PDI of L-SL  
205 changed considerably from 0.408 to 0.258 at month 7, coinciding with the most pronounced  
206 decrease in z-average.

207

### 208 **3.2. Moisture and water solubility**

209 The moisture content decreased in all the dried liposomes without significant differences  
210 depending on the entrapped compound (Table 2). Ye et al. (2017) reported a water content  
211  $< 15\%$  for all their freeze-dried liposomes. The higher hydration level observed in the present  
212 work could be attributed to the use of glycerol for liposome production, in agreement with  
213 Manca et al. (2013). The highly hygroscopic nature of glycerol inhibited the formation of a dry

214 lyophilized powder, providing samples with a gluey and pasty texture, as reported previously  
215 (Taladrid et al., 2017). Unlike the empty liposome, moisture content was significantly ( $p \leq 0.05$ )  
216 reduced in the freeze-dried liposomes loaded with the various natural compounds within the  
217 first 3 months of storage and thereafter. The rearrangement of residual water molecules in the  
218 first stages of frozen storage could cause destabilization of water interactions with glycerol in  
219 the presence of the entrapped compounds, probably favouring water evaporation during  
220 moisture content determination. This finding provides first indication that the entrapped  
221 compounds could cause structural changes in the liposomal membrane.

222 The fresh L-E suspension had a water solubility significantly lower ( $p \leq 0.05$ ) than in L-HC, L-PG  
223 and L-SL (Table 2). This difference might reflect structural changes in the membrane bilayer  
224 resulting from interactions with the entrapped compounds that led to a decrease in vesicle  
225 aggregation. When the liposomes were freeze-dried, a pronounced decrease in water  
226 solubility was found in L-SL, indicating higher vesicle aggregation.

227

### 228 **3.3. Entrapment efficiency**

229 Immediately after freeze-drying, the entrapment efficiency for L-HC, L-PG and L-SL was,  
230 respectively, 87%, 63% and 97% (Table 3). The EE in all the formulations remained stable  
231 ( $p > 0.05$ ) during 7 months of storage, in agreement with Laverman et al. (2000) for freeze-dried  
232 liposomes stored for one year.

233 The higher entrapment in L-SL was attributed to the lipid nature of the shrimp extract, which  
234 enabled greater allocation within the fatty acid acyl chains of the membrane bilayer. Because  
235 of the poor water solubility of SL, it was more difficult for it to leak out from the liposomes  
236 upon rehydration (Chen et al., 2010). In the liposomes loaded with HC and PG, their  
237 hydrophilic components would be mostly entrapped in the inner aqueous core of the

238 liposome. In the case of L-PG, the lower EE would indicate that a considerable amount of  
239 phenolic compounds remained outside the vesicles. Subsequent changes in membrane fluidity  
240 during the storage period could be responsible for the size reduction in all the preparations,  
241 but they did not cause leakage of the entrapped compounds.

242

### 243 **3.4. Colour**

244 Freeze-dried L-E and L-HC samples showed higher ( $p \leq 0.05$ ) values of luminosity ( $L^*$ ) and  
245 yellowness ( $b^*$ ) than L-PG and L-SL (Table 4). Parameter  $a^*$  (redness) was highest for L-SL.  
246 Encapsulation of the collagen hydrolysate caused very slight changes in liposome coloration,  
247 the appearance changing from yellowish in L-E to light brown in L-HC. The pomegranate  
248 extract caused notable darkening in L-PG, probably due to the remaining non-encapsulated  
249 extract in this sample. The noticeable orange colour in L-SL (hue angle of  $39^\circ$ ) was attributed to  
250 the carotenoid content in the shrimp lipid extract (Gómez-Estaca et al., 2017). According to  
251 Hama et al. (2012), the preferential location of the astaxanthin terminal rings on the liposomal  
252 membrane surface could be mainly responsible for the orange colour of the L-SL sample. The  
253 colour parameters of the various freeze-dried liposomes did not change during the storage  
254 time (data not shown).

255

### 256 **3.5. Cryo-transmission electron microscopy**

257 The cryo-TEM images of fresh liposomes showed similar morphology and particle size  
258 distribution for empty and loaded liposomes, most of them being spherical, well-separated  
259 unilamellar vesicles, although a few liposomes showed a bivesicular configuration (Figure 1).  
260 The vesicles had different sizes, according to the polydispersity shown in Table 1, with a  
261 greater abundance of small vesicles than of large ones. The freeze-dried L-HC and L-PG

262 liposomes showed large multivesicular vesicles, more pronouncedly in L-PG, without losing  
263 their characteristic spherical and unilamellar morphology (Figure 2). In the L-SL paste, large  
264 multilamellar vesicles and also morphologies with a varying degree of invagination were  
265 observed.

266

### 267 **3.6. Differential scanning calorimetry**

268 DSC results of fresh liposomal suspensions and freeze-dried pastes are presented in Figure 3  
269 and Table 5. Liposome suspensions were characterised by a highly cooperative endothermic  
270 transition at sub-zero temperatures ( $T_{\text{peak1}}$ ). L-HC, L-PG and L-SL exhibited a slight increase  
271 ( $p \leq 0.05$ ) in  $T_{\text{peak1}}$  as compared to the empty liposomes. The inclusion of the extracts increased  
272 ( $p \leq 0.05$ ) the enthalpy ( $\Delta H$ ) by around 39–43% with respect to the empty liposomes, in  
273 agreement with previous work on asolectin-genistein liposomes (Lopes de Azambuja et al.,  
274 2015). Fresh empty liposomes (L-E) showed a second minor endothermic event ( $T_{\text{peak2}}$ ) at 10.8  
275 °C ( $\Delta H = 2.97$  J/g), which was not observed in the other liposomal preparations within the  
276 range of temperatures tested (–30 to 90 °C). These findings indicated structural changes in the  
277 membrane bilayer, probably owing to interactions of the entrapped compounds with the polar  
278 head groups and their intercalation in the bilayer membrane.

279 The DSC traces of the freeze-dried pastes showed more diffuse endothermic transitions as a  
280 result of the reduced moisture content (Figure 3b, Table 5). The main transition shifted to 4 °C  
281 in L-E, 2 °C in L-HC and L-PG, and 11 °C in L-SL, with very weak enthalpy values (data not  
282 shown). The increase in the main  $T_m$  of the lipid membrane upon lyophilisation was ascribed  
283 to decreased head group spacing causing large compressive stress in the lipids in the dry state  
284 (Koster, Lei, Anderson, Martin & Bryant, 2000). The higher  $T_{\text{peak}}$  in the dried form of L-SL would  
285 indicate that the predominant liposoluble compounds in the shrimp extract (namely fatty  
286 acids, tocopherol, astaxanthin and cholesterol) were strongly embedded inside the lipid

287 bilayer, contributing to an increase in the stability of the liposomal membrane. In particular,  
288 cholesterol has been widely reported as an active agent providing rigidity and stability to  
289 phosphatidylcholine bilayer membranes (Sułkowski et al., 2005). The presence of large  
290 multilamellar vesicles in L-SL after freeze-drying would also contribute to an increase in the  
291 thermal stability. The transition temperature in L-E showed a progressive decrease during the  
292 storage period. A significant decrease ( $p \leq 0.05$ ) was also found in L-HC after seven months of  
293 storage. In contrast,  $T_{\text{peak}}$  of L-PG and L-SL pastes remained unchanged ( $p > 0.05$ ) during the  
294 whole storage period.

295

### 296 **3.7. Infrared spectroscopy (ATR-FTIR)**

297 Infrared spectroscopy was used to evaluate structural and conformational changes caused by  
298 entrapment of the various compounds at different parts of the bilayer (Toyran et al., 2003).  
299 Figure 4 depicts changes in frequency peaks immediately after freeze-drying and after 3 and 7  
300 months of frozen storage.

301 Variations in wavenumbers at  $\approx 2925 \text{ cm}^{-1}$  and  $\approx 2850 \text{ cm}^{-1}$ , related respectively to  $\text{CH}_2$   
302 asymmetric and symmetric stretching vibrations, revealed changes occurring in the bilayer acyl  
303 chains. The downshift in the  $2925 \text{ cm}^{-1}$  band in newly freeze-dried liposomes was only  
304 observed in L-SL, indicative of greater stiffness in the deep interior of the bilayer (Figure 4a).  
305 The lipophilic nature of the SL caused an ordering effect through hydrophobic interactions with  
306 the membrane acyl chains, in agreement with reported work on liposomes loaded with  
307 different hydrophobic compounds (Toyran et al., 2003; Lopes de Azambuja et al., 2015;  
308 Pawlikowska-Pawłęga et al., 2014). This finding was in agreement with the higher thermal  
309 transition temperature observed by DSC. The apparent lack of intercalation into the aliphatic  
310 chain zone of the phenolic PG extract in the present study could be due to its lower  
311 hydrophobic nature in comparison with pure flavonoids used in other works, and also to the

312 relatively low entrapment efficiency. The storage period shifted the peak frequency at  $\approx 2925$   
313  $\text{cm}^{-1}$  towards lower values in all the liposomes, indicating an increase in membrane rigidity,  
314 which coincided with the particle size reduction in all the freeze-dried liposomes during  
315 storage.

316 Slight variations were observed in the C=O stretching absorption band at  $\approx 1740 \text{ cm}^{-1}$  (Figure  
317 4b), related to structural changes associated with the hydration state of carbonyl groups at the  
318 interfacial part of the membrane (Toyran et al., 2003). Loading with the various extracts hardly  
319 altered the peak frequency with respect to the empty liposomes, indicating little interaction of  
320 the loaded compounds with the ester carbonyl groups. The decrease in peak frequency at  
321  $\approx 1740 \text{ cm}^{-1}$  during storage in L-SL and L-PG might indicate variable interactions of the loaded  
322 compounds at this membrane level. However, the downshift also observed in L-E at month 7  
323 suggested that the dehydration of carbonyl groups could also be a result of intrinsic structural  
324 changes in the membrane.

325 The  $\text{PO}_2^-$  antisymmetric double bond stretching at  $\approx 1220 \text{ cm}^{-1}$  revealed information related to  
326 the phospholipid polar head groups of the membrane (Figure 4c). The upwards shift observed  
327 in all the loaded liposomes as compared to the empty ones indicated a noticeable reduction in  
328 the hydration state of the phosphate groups as a result of strong hydrogen bonding with the  
329 various extracts, in descending order, L-SL, L-PG and L-HC. A similar FTIR event was reported in  
330 liposomes loaded with genistein (Lopes de Azambuja et al., 2015). The stronger dehydration at  
331 the membrane surface observed in the L-SL preparation coincided with higher vesicle  
332 aggregation resulting from freeze-drying (lower water solubility). After 3 months of storage of  
333 L-E and L-HC, and 7 months in the case of L-PG, a considerable increase in the peak frequency  
334 at  $\approx 1220 \text{ cm}^{-1}$  was observed, which did not occur in L-SL. The greater stiffness in the deep  
335 interior of the bilayer and strong hydrogen bonding with polar head groups in L-SL probably  
336 restricted conformational changes in the course of time.

337

### 338 **3.8. Rheological properties**

339 The mechanical spectra representing the frequency dependence of the elastic ( $G'$ ) and viscous  
340 ( $G''$ ) moduli immediately after freeze-drying are shown in Figure 5. All spectra fitted the power  
341 law model ( $R^2 > 0.99$ ), presented slightly higher values of  $G''$  than  $G'$ , and phase angle  $>45^\circ$ .

342 These results indicated that the dried liposomal pastes presented viscoelastic behaviour typical  
343 of a highly viscous fluid rather than a solid material, attributed to the plasticizing effect of  
344 glycerol. This property makes them suitable to be incorporated as functional ingredients in  
345 restructured meat or fish products. The viscoelastic parameters of the freeze-dried pastes at 1  
346 Hz and the value of the exponent  $n'$ , obtained from fitting the mechanical spectra of  $G'$  to the  
347 power law equation are presented in Figure 6. The entrapment with the various extracts led to  
348 an increase in both  $G'$  and  $G''$ , without noticeable changes in the phase angle. These results  
349 indicate that the loaded freeze-dried liposomes became harder without substantially changing  
350 their viscoelastic nature. This effect was attributed to interactions of the entrapped  
351 compounds with the membrane polar head groups. The structural stability of the liposomal  
352 pastes was determined from the value of the power law exponent ( $n'$ ): the higher the  $n'$   
353 values, the higher the instability of the matrix against frequency changes. The  $n'$  was highest  
354 ( $p \leq 0.5$ ) in L-PG, indicating greater matrix discontinuity. The viscous modulus ( $G''$ ) in L-PG was  
355 much greater than in the other preparations. These effects could be due to the lower  
356 entrapment efficiency determined in L-PG, in which the non-encapsulated compounds would  
357 have slightly hindered interactions among the dried lipid vesicles. This finding agrees with the  
358 higher water solubility of this sample immediately after freeze-drying (Table 2).

359 After 7 months of storage, all samples, except L-PG, showed noticeably higher  $G'$  and  $G''$   
360 values, L-E being the preparation that registered the most pronounced increase. These results  
361 indicate that the liposomal pastes tended to harden during the storage period, in agreement

362 with the increase in membrane rigidity as observed by FTIR. Changes in phase angle and in  $n'$   
363 were rather low, so the viscoelastic nature of the liposomal pastes did not change substantially  
364 with storage time. In the case of L-PG the sample hardening was not clearly evidenced, but the  
365 slight reduction of phase angle and  $n'$  suggested a slight increase in matrix stability.

366 All preparations presented a decreasing tendency in  $G'$  and  $G''$  with the rise in temperature,  
367 with the exception of L-SL (Figure 7). This loss of consistency could be due to the heat-induced  
368 disruption of interactions responsible for adhesion forces between adjacent lipid bilayers and  
369 also between lipids within the bilayer (Augustyńska et al., 2016). Temperature plays a key role  
370 in modifying local lipid orientation and producing a less ordered lipid arrangement, with the  
371 result that inner interactions would be weakened. Tan et al. (2013) reported a heat-induced  
372 decrease in the microviscosity of egg yolk phosphatidylcholine liposomes associated with a  
373 decrease in membrane fluidity when the temperature increased above 50 °C.

374 The L-SL sample showed a pronounced increase in  $G'$  from 40 °C to 90 °C, indicating the  
375 formation of a strong heat-induced gel-like structure. The SL extract stabilized the membrane  
376 mechanical strength and favoured resistance to rupture at high temperatures. Similar findings  
377 were obtained by Augustyńska et al. (2016) for liposomes encapsulating  $\beta$ -carotene. Tan et al.  
378 (2013) demonstrated that the incorporation of lutein enhanced membrane rigidity by  
379 restricting the motion freedom of lipids through interactions with lutein molecules. In  
380 particular, hydrophobic interactions were reported to be the main reason for the structural  
381 stability of the lipid bilayer upon heating up to 80 °C. In the present work, the sharp heat-  
382 induced rigidifying effect observed when heating above 40 °C in L-SL suggested a  
383 predominance of thermostable hydrophobic interactions occurring at high temperatures. The  
384 thermal behaviour of the various liposomal preparations remained practically the same during  
385 long-term storage, but registering higher values of  $G'$  and  $G''$  from the onset of heating. This  
386 effect was probably the result of increased adhesion forces between lipid vesicles and also an



387 increase in membrane stiffness with time. However, the mainly responsible interactions kept  
388 their susceptibility to heat-induced breakdown. In the case of L-SL above 40 °C, the  
389 hydrophobic heat-induced interactions still helped to form an even stronger gel-like structure,  
390 as compared to that obtained immediately after-freeze-drying.

391

### 392 **3.9. Lipid oxidation**

393 The phosphatidylcholine (PC) used in this work is highly unsaturated, with linoleic acid  
394 accounting for ≈59% of the total fatty acids (Taladrid et al., 2017). The predominance of  
395 polyunsaturated fatty acids may generate hydroperoxides and secondary oxidation products  
396 leading to the accumulation of TBARS in soy lecithin emulsions (Wang and Wang, 2008). The  
397 MDA equivalent content in all the liposomal preparations is shown in Table 2. For the fresh  
398 liposomal suspensions, all TBARS were very low (8.22–18.4 µg/kg, expressed on a dry basis).  
399 The MDA equivalent content determined in the raw phosphatidylcholine ( $22.63 \pm 0.86$  µg/kg)  
400 was slightly higher than in the fresh liposomes, probably because the formation of the lipid  
401 bilayer limited the interaction of the reactive substances with the TBA. Therefore, no  
402 perceptible accumulation of secondary products of lipid oxidation could be attributed to the  
403 liposome preparation procedure. It should be noted that the PC used for liposome production  
404 presented significant residual amounts of tocopherol species, including  $\alpha$ -tocopherol (Taladrid  
405 et al., 2017), which is a well-recognized antioxidant.

406 The TBARS increased ( $p \leq 0.05$ ) in all freeze-dried liposomes probably favoured by structural  
407 and conformational changes in the bilayer that might have increased the exposure of  
408 hydrophobic compartments to the environment. Oxygen and free radicals are more soluble in  
409 the fluid lipid bilayer than in the aqueous solution. In particular, the presence of dihydrogen  
410 phosphate ions in the phosphate buffer solution was reported to decrease oxygen solubility  
411 and associated liposome oxidation (Guner & Oztop, 2017). Thus, oxygen concentration in the

412 interior organic phase of the membrane upon dehydration would have probably promoted  
413 lipid oxidation (Pamplona, 2008).

414 At this time, L-PG was the liposome with the lowest MDA equivalent content, while L-E had the  
415 highest one. The higher MDA equivalent content in L-E suggested that the loading with  
416 antioxidant compounds could prevent some lipid oxidation after freeze-drying. The inhibition  
417 of lipid peroxidation might be a consequence of the combination of two mechanisms: (1) the  
418 intrinsic antioxidant property of the added compounds, and (2) their effects on the membrane  
419 properties by limiting molecular oxygen penetration into the lipid bilayer (Tan et al., 2013). The  
420 extracts used in the present study have been reported to have antioxidant capacity, which is  
421 normally higher in the case of phenolic compounds, carotenoids and tocopherol than in  
422 collagen hydrolysates (Alemán et al., 2011; Gómez-Estaca et al., 2017; Masci et al., 2016).  
423 Probably for this reason, the prevention of freeze-drying-induced TBARS accumulation was  
424 significantly lower in L-HC as compared to L-PG or L-SL. During the 7 months of storage the  
425 TBARS value gradually decreased ( $p \leq 0.05$ ) in all cases, with L-SL having the lowest values at the  
426 end of the storage time. The unexpected reduction in TBARS values could be indicative of lipid  
427 oxidative instability. A great diversity of phospholipid oxidation products and aldehydes are  
428 generated during lipid peroxidation of polyunsaturated fatty acids (Catalá, 2009). Some of  
429 them are very reactive and unstable molecules, so that their presumptive interaction with  
430 liposome phospholipids would explain the decline in measured TBARS. Signs of lipid oxidation  
431 in freeze-dried empty liposomes during the storage time, observed by FTIR, are shown in  
432 Figure 8. The progressive decrease in the intensity absorbance in the region between 3600 and  
433  $3100 \text{ cm}^{-1}$  with the concomitant increase and broadening of the band at  $\approx 1740 \text{ cm}^{-1}$ , would be  
434 indicative of progressive decomposition of hydroperoxides to yield aldehydes and ketones. The  
435 band at  $\approx 1740 \text{ cm}^{-1}$  was already proposed as useful infrared marker of the formation of  
436 secondary lipid oxidation products in liposomes (Lamba et al., 1991). Similar behaviour was  
437 found in freeze-dried liposomes entrapping the various compounds (data not shown),

438 indicating that lipid oxidation was not efficiently prevented during storage, even at frozen  
439 conditions.

440

### 441 **3.10. Conclusions**

442 The freeze-drying process caused structural changes in the membrane bilayer depending on  
443 the chemical nature of the entrapped compounds and their encapsulation efficiency. The  
444 loading with the various extracts did not negatively affect the mechanical stability of the  
445 freeze-dried liposomes during storage and prevented lipid oxidation. Liposomes loaded with  
446 lipophilic compounds may suffer a strong heat-induced rigidifying effect which should be  
447 considered in thermally treated foods. Dry liposomes entrapping bioactive compounds could  
448 serve as potential ingredients with long-term storage stability for designing functional food  
449 products with low or intermediate moisture level. To avoid oxidative instability of freeze-dried  
450 liposomes, various strategies could be proposed, such as optimization of the freeze-drying  
451 procedure or further membrane stabilization with amphiphilic antioxidants.

452

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457

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568



569 FIGURE CAPTIONS

570 FIGURE 1. Cryo-TEM images of fresh liposomes: (a) L-E: empty liposomes; (b) L-HC: liposomes  
571 with collagen hydrolysate; (c) L-PG: liposomes with pomegranate extract; (d) L-SL: liposomes  
572 with shrimp lipid extract.

573

574 FIGURE 2. Cryo-TEM images of newly freeze-dried liposomal pastes: (a) L-HC: liposomes with  
575 collagen hydrolysate; (b) L-PG: liposomes with pomegranate extract; (c) L-SL: liposomes with  
576 shrimp lipid extract.

577

578 FIGURE 3. DSC traces of: (a) fresh liposomal suspensions; (b) newly freeze-dried liposomal  
579 pastes.

580 L-HC: liposomes with collagen hydrolysate; L-PG: liposomes with pomegranate extract; L-SL:  
581 liposomes with shrimp lipid extract.

582

583 FIGURE 4. Frequency variations in stretching modes of selected functional groups determined  
584 in freeze-dried liposomal pastes: (a)  $\text{CH}_2$  asymmetric stretching vibration; (b) C=O stretching  
585 vibration; (c)  $\text{PO}_2^-$  antisymmetric double bond stretching vibration.

586 L-HC: liposomes with collagen hydrolysate; L-PG: liposomes with pomegranate extract; L-SL:  
587 liposomes with shrimp lipid extract.

588

589 FIGURE 5. Mechanical spectra of newly freeze-dried liposomal pastes: (a) Elastic modulus ( $G'$ ,  
590 Pa); (b) Viscous modulus ( $G''$ , Pa).

591 L-HC: liposomes with collagen hydrolysate; L-PG: liposomes with pomegranate extract; L-SL:  
592 liposomes with shrimp lipid extract.

593

594 FIGURE 6. Viscoelastic parameters, determined at 1 Hz, of the newly freeze-dried liposomal  
595 pastes and pastes stored for 7 months: (a) Elastic modulus ( $G'$ , Pa); (b) Viscous modulus ( $G''$ ,  
596 Pa); (c) phase angle ( $\delta$ , °); (d) power law exponent ( $n'$ ).

597 L-HC: liposomes with collagen hydrolysate; L-PG: liposomes with pomegranate extract; L-SL:  
598 liposomes with shrimp lipid extract.

599

600 FIGURE 7. Viscoelastic properties as a function of temperature of the newly freeze-dried  
601 liposomal pastes: (a) Elastic modulus ( $G'$ , Pa), (b) Viscous modulus ( $G''$ , Pa); and pastes stored  
602 for 7 months: (c) Elastic modulus ( $G'$ , Pa), (d) Viscous modulus ( $G''$ , Pa).

603 L-HC: liposomes with collagen hydrolysate; L-PG: liposomes with pomegranate extract; L-SL:  
604 liposomes with shrimp lipid extract.

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Table 1. Particle size (expressed as z-average), polydispersity index (PDI) and zeta potential of fresh liposomes stored for 2 weeks at 4 °C and freeze-dried liposomes stored for 7 months at –20 °C.

		Fresh			Freeze-dried		
		0 weeks	1 weeks	2 weeks	0 months	3 months	7 months
z-average (nm)	L-E	87.4±0.8 <sup>B/M</sup>	85.7±0.0 <sup>A/M</sup>	86.2±0.9 <sup>A,B/M</sup>	316.6±6.7 <sup>c/N</sup>	261.0±3.5 <sup>b/P</sup>	159.0±2.7 <sup>a/M</sup>
	L-HC	102.3±0.8 <sup>A/N</sup>	104.2±1.1 <sup>B/N</sup>	104.7±0.4 <sup>B/N</sup>	274.9±5.5 <sup>b/M</sup>	183.3±2.0 <sup>a/O</sup>	177.4±2.6 <sup>a/N</sup>
	L-PG	104.2±0.8 <sup>A/N</sup>	104.0±0.9 <sup>A/N</sup>	105.5±0.8 <sup>A/N</sup>	256.8±2.3 <sup>b/M</sup>	174.5±3.6 <sup>a/N</sup>	178.2±2.3 <sup>a/N</sup>
	L-SL	102.2±1.6 <sup>A/N</sup>	105.0±0.8 <sup>A,B/N</sup>	107.0±1.7 <sup>B/N</sup>	372.9±15.9 <sup>b/O</sup>	150.0±0.6 <sup>a/M</sup>	159.2±2.4 <sup>a/M</sup>
PDI	L-E	0.240±0.005 <sup>A/M</sup>	0.241±0.007 <sup>A/M</sup>	0.230±0.007 <sup>A/M</sup>	0.374±0.081 <sup>a/M</sup>	0.316±0.035 <sup>a/N</sup>	0.368±0.018 <sup>a/N</sup>
	L-HC	0.247±0.019 <sup>A/M</sup>	0.256±0.007 <sup>A/M</sup>	0.256±0.006 <sup>A/M,N</sup>	0.334±0.033 <sup>a,b/M</sup>	0.386±0.012 <sup>b/O</sup>	0.311±0.033 <sup>a/M</sup>
	L-PG	0.263±0.017 <sup>A/M</sup>	0.263±0.008 <sup>A/M</sup>	0.264±0.016 <sup>A/N</sup>	0.279±0.021 <sup>a/M</sup>	0.319±0.021 <sup>a/N</sup>	0.293±0.026 <sup>a/M</sup>
	L-SL	0.246±0.017 <sup>A/M</sup>	0.254±0.015 <sup>A/M</sup>	0.264±0.015 <sup>A/N</sup>	0.408±0.112 <sup>a/M</sup>	0.264±0.009 <sup>a/M</sup>	0.258±0.005 <sup>a/M</sup>
Zeta potential (mV)	L-E	-35.5±1.7 <sup>B/N</sup>	-38.9±1.1 <sup>A,B/M</sup>	-43.7±3.7 <sup>A/M</sup>	-54.2±1.5 <sup>a/N</sup>	-47.8±1.2 <sup>b/M,N</sup>	-45.5±1.0 <sup>b/M</sup>
	L-HC	-43.4±0.7 <sup>A/M</sup>	-41.5±1.7 <sup>A/M</sup>	-31.7±0.6 <sup>B/O</sup>	-54.9±0.7 <sup>a/N</sup>	-50.8±1.8 <sup>b/M</sup>	-49.8±1.2 <sup>b/N</sup>
	L-PG	-38.2±0.7 <sup>A/N</sup>	-40.4±1.8 <sup>A/M</sup>	-38.8±0.7 <sup>A/N</sup>	-57.2±0.5 <sup>a/M,N</sup>	-45.2±2.1 <sup>b/N</sup>	-46.6±2.1 <sup>b/M,N</sup>
	L-SL	-41.9±2.2 <sup>A/M</sup>	-41.2±0.8 <sup>A/M</sup>	-32.9±0.7 <sup>B/O</sup>	-59.1±2.2 <sup>a/M</sup>	-44.1±1.1 <sup>b/N</sup>	-47.5±1.8 <sup>b/M,N</sup>

L-E: empty liposomes; L-HC: liposomes with collagen hydrolysate; L-PG: liposomes with pomegranate extract; L-SL: liposomes with shrimp lipids extract. Different letters (A, B) indicate significant differences ( $p \leq 0.05$ ) in fresh liposomes as a function of time. Different letters (a, b, c) indicate significant differences ( $p \leq 0.05$ ) in freeze-dried liposomes as a function of time. Different letters (M, N, O, P) indicate significant differences ( $p \leq 0.05$ ) among liposome formulations.

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Table 2. Moisture content, water solubility and thiobarbituric acid reactive substances (TBARS) of newly fresh liposomes and freeze-dried liposomes stored for 7 months at  $-20\text{ }^{\circ}\text{C}$ .

		Fresh		Freeze-dried	
		0 weeks	0 months	3 months	7 months
Moisture (%)	L-E	$91.97 \pm 0.57^{\text{M}}$	$18.48 \pm 2.20^{\text{a/M}}$	$16.60 \pm 2.38^{\text{a/N}}$	$17.06 \pm 1.33^{\text{a/M}}$
	L-HC	$92.75 \pm 0.27^{\text{M}}$	$21.30 \pm 1.10^{\text{b/M}}$	$10.03 \pm 2.30^{\text{a/M}}$	$11.74 \pm 2.29^{\text{a/M}}$
	L-PG	$92.65 \pm 0.36^{\text{M}}$	$24.39 \pm 2.64^{\text{b/M}}$	$10.27 \pm 2.36^{\text{a/M}}$	$15.12 \pm 4.33^{\text{a/M}}$
	L-SL	$92.77 \pm 0.50^{\text{M}}$	$24.87 \pm 4.55^{\text{b/M}}$	$10.09 \pm 1.78^{\text{a/M}}$	$18.62 \pm 4.11^{\text{b/M}}$
Solubility (%)	L-E	$74.34 \pm 11.49^{\text{M}}$	$73.63 \pm 2.62^{\text{a/N}}$	$73.54 \pm 0.69^{\text{a/N}}$	$73.56 \pm 1.77^{\text{a/N}}$
	L-HC	$87.36 \pm 3.98^{\text{M}}$	$76.45 \pm 0.37^{\text{a/N}}$	$74.51 \pm 1.53^{\text{a/N}}$	$87.12 \pm 2.50^{\text{b/N}}$
	L-PG	$83.90 \pm 3.93^{\text{M}}$	$80.90 \pm 1.66^{\text{a/O}}$	$78.64 \pm 3.59^{\text{a/N}}$	$85.25 \pm 13.17^{\text{a/N}}$
	L-SL	$87.60 \pm 3.99^{\text{M}}$	$65.22 \pm 1.33^{\text{b/M}}$	$49.69 \pm 4.19^{\text{a/M}}$	$56.24 \pm 5.77^{\text{a,b/M}}$
TBARS ( $\mu\text{g}$ MDA eq/kg dry matter)	L-E	$8.22 \pm 1.94^{\text{M}}$	$81.8 \pm 3.56^{\text{M/a}}$	$65.2 \pm 1.29^{\text{M/b}}$	$38.5 \pm 0.70^{\text{M/c}}$
	L-HC	$18.4 \pm 2.10^{\text{O}}$	$69.2 \pm 2.97^{\text{N/a}}$	$44.2 \pm 1.25^{\text{N/b}}$	$32.3 \pm 1.30^{\text{N/c}}$
	L-PG	$9.80 \pm 0.00^{\text{MN}}$	$46.6 \pm 2.86^{\text{P/a}}$	$24.7 \pm 5.89^{\text{P/b}}$	$23.5 \pm 1.23^{\text{O/b}}$
	L-SL	$12.4 \pm 1.05^{\text{N}}$	$58.5 \pm 4.74^{\text{O/a}}$	$33.3 \pm 4.31^{\text{O/b}}$	$15.5 \pm 0.29^{\text{P/c}}$

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L-E: empty liposomes; L-HC: liposomes with collagen hydrolysate; L-PG: liposomes with pomegranate extract; L-SL: liposomes with shrimp lipid extract. Different letters (M, N, O, P) indicate significant differences ( $p \leq 0.05$ ) among liposome formulations. Different letters (a, b, c) indicate significant differences ( $p \leq 0.05$ ) in freeze-dried liposomes as a function of time.

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Table 3. Entrapment efficiency of freeze-dried liposomes stored for 7 months at  $-20\text{ }^{\circ}\text{C}$ .

	Entrapment efficiency (%)		
	0 months	3 months	7 months
L-HC	$87.25 \pm 1.97^{a/M}$	$86.61 \pm 5.08^{a/M}$	$89.60 \pm 2.20^{a/M}$
L-PG	$63.19 \pm 3.90^{a/N}$	$62.88 \pm 1.71^{a/N}$	$62.44 \pm 3.03^{a/N}$
L-SL	$97.24 \pm 0.08^{a/M}$	$96.92 \pm 0.00^{a/M}$	$96.96 \pm 0.09^{a/M}$

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L-HC: liposomes with collagen hydrolysate; L-PG: liposomes with pomegranate extract; L-SL: liposomes with shrimp lipid extract. Different letters (M, N, O, P) indicate significant differences ( $p \leq 0.05$ ) among liposome formulations. Different letters (a, b, c) indicate significant differences ( $p \leq 0.05$ ) as a function of time.

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Table 4. Colour parameters of newly freeze-dried liposomes

	Colour parameters				
	L*(D65)	a*(D65)	b*(D65)	Chroma	Hue angle (°)
L-E	32.52 ± 0.22 <sup>A</sup>	0.95 ± 0.09 <sup>A</sup>	8.27 ± 0.14 <sup>A</sup>	8.32 ± 0.15 <sup>A</sup>	83.46 ± 0.53 <sup>A</sup>
L-HC	32.71 ± 0.22 <sup>A</sup>	3.23 ± 0.20 <sup>B</sup>	10.54 ± 0.18 <sup>B</sup>	11.02 ± 0.22 <sup>B</sup>	72.99 ± 0.80 <sup>B</sup>
L-PG	27.81 ± 0.22 <sup>B</sup>	2.33 ± 0.07 <sup>C</sup>	5.27 ± 0.27 <sup>C</sup>	5.76 ± 0.27 <sup>C</sup>	66.12 ± 0.79 <sup>C</sup>
L-SL	29.06 ± 0.25 <sup>C</sup>	7.10 ± 0.21 <sup>D</sup>	5.80 ± 0.22 <sup>D</sup>	9.17 ± 0.30 <sup>D</sup>	39.25 ± 0.45 <sup>D</sup>

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L-HC: liposomes with collagen hydrolysate; L-PG: liposomes loaded pomegranate extract; L-SL: liposomes with shrimp lipid extract. Different letters (A, B, C, ...) indicate significant differences ( $p \leq 0.05$ ) among liposome formulations.

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643 Table 5. Transition temperatures and enthalpy  
644 changes in fresh and freeze-dried liposomes  
645 stored for 7 months at  $-20\text{ }^{\circ}\text{C}$ .

	$T_{\text{peak 1}}$ ( $^{\circ}\text{C}$ )	Enthalpy (J/g)
<u>Fresh</u>		
L-E	$-6.59 \pm 0.20^{\text{a}}$	$120.6 \pm 0.64^{\text{a}}$
L-HC	$-3.91 \pm 0.40^{\text{bc}}$	$171.6 \pm 0.07^{\text{bcd}}$
L-PG	$-4.24 \pm 0.66^{\text{b}}$	$161.8 \pm 4.38^{\text{b}}$
L-SL	$-4.29 \pm 0.35^{\text{b}}$	$166.8 \pm 3.81^{\text{bc}}$
<u>Dry – 0 months</u>		
L-E	$3.98 \pm 1.06^{\text{a}}$	-
L-HC	$2.04 \pm 0.50^{\text{b}}$	-
L-PG	$1.76 \pm 0.47^{\text{b}}$	-
L-SL	$11.05 \pm 0.93^{\text{c}}$	-
<u>Dry – 3 months</u>		
L-E	$0.85 \pm 0.86^{\text{bd}}$	-
L-HC	$1.15 \pm 0.92^{\text{b}}$	-
L-PG	$0.88 \pm 0.08^{\text{b}}$	-
L-SL	$9.69 \pm 0.38^{\text{c}}$	-
<u>Dry – 7 months</u>		
L-E	$-0.53 \pm 0.27^{\text{de}}$	-
L-HC	$-1.30 \pm 0.48^{\text{e}}$	-
L-PG	$1.66 \pm 0.00^{\text{b}}$	-
L-SL	$10.19 \pm 0.13^{\text{c}}$	-

646 L-E: empty liposomes; L-HC: liposomes with collagen  
647 hydrolysate; L-PG: liposomes with pomegranate extract; L-SL:  
648 liposomes with shrimp lipid extract. Different letters (a, b, c,  
649 ...) indicate significant differences ( $p \leq 0.05$ ) as a function of  
650 liposome formulation and time.

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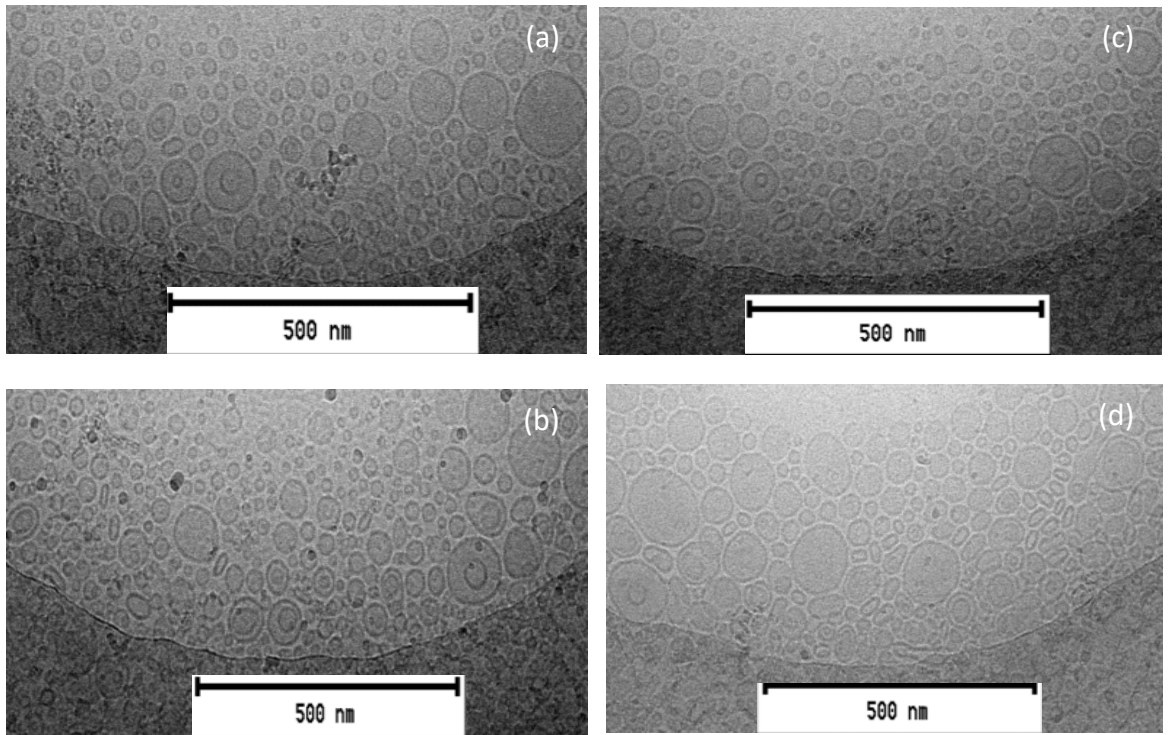


FIGURE 1. Cryo-TEM images of fresh liposomes: (a) L-E: empty liposomes; (b) L-HC: liposomes with collagen hydrolysate; (c) L-PG: liposomes with pomegranate extract; (d) L-SL: liposomes with shrimp lipid extract

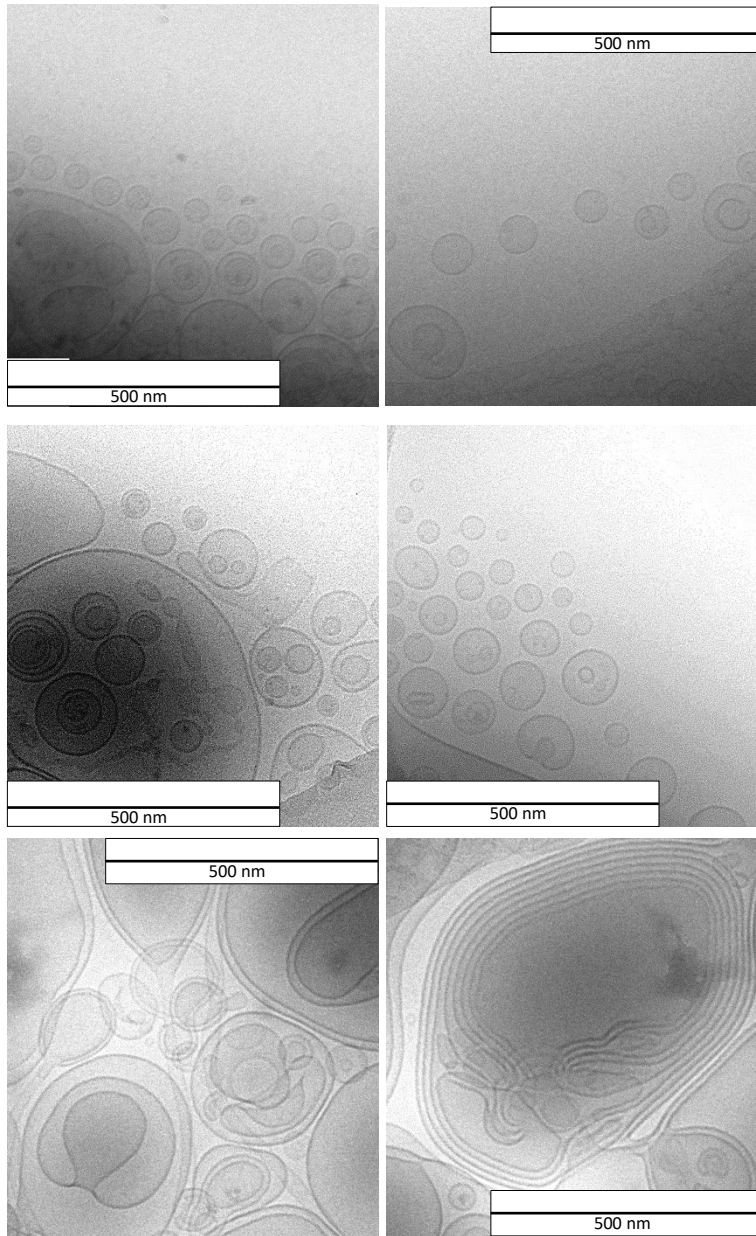


FIGURE 2. Cryo-TEM images of newly freeze-dried liposomal pastes:  
(a) L-HC: liposomes with collagen hydrolysate; (b) L-PG: liposomes with  
(b) pomegranate extract; (c) L-SL: liposomes with shrimp lipid extract.



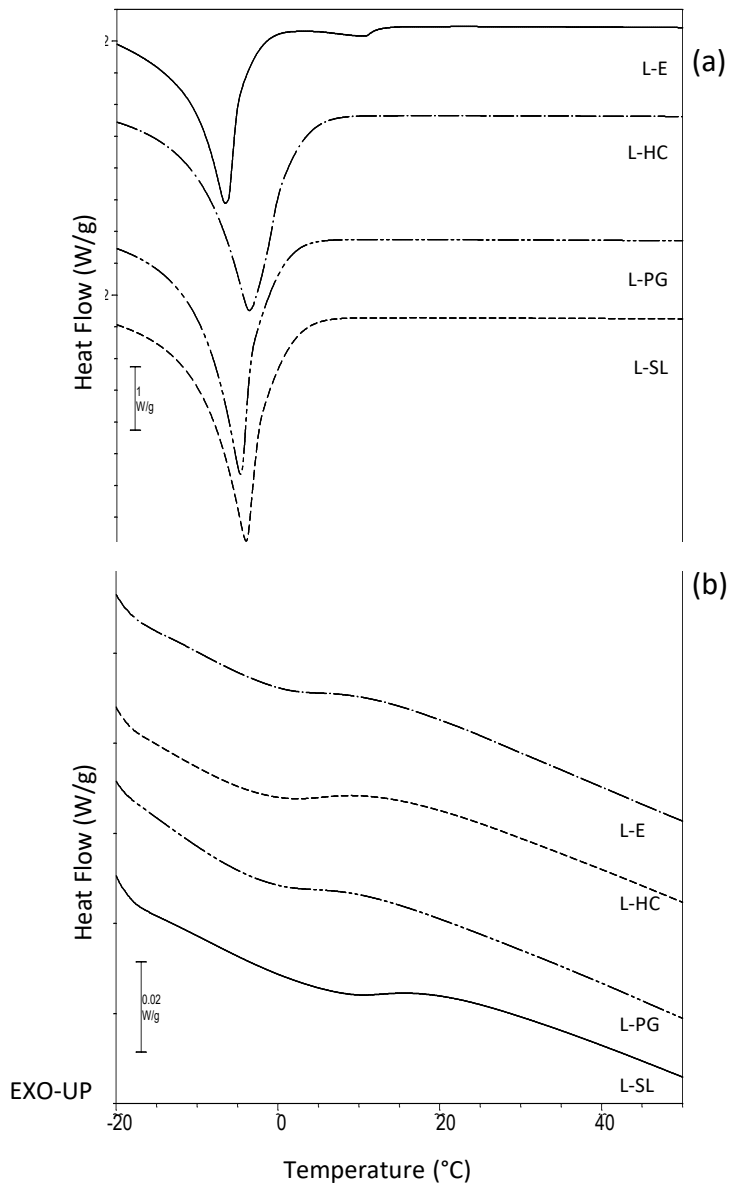


FIGURE 3. DSC traces of: (a) fresh liposomal suspensions; (b) newly freeze-dried liposomal pastes. L-HC: liposomes with collagen hydrolysate; L-PG: liposomes with pomegranate extract; L-SL: liposomes with shrimp lipid extract.

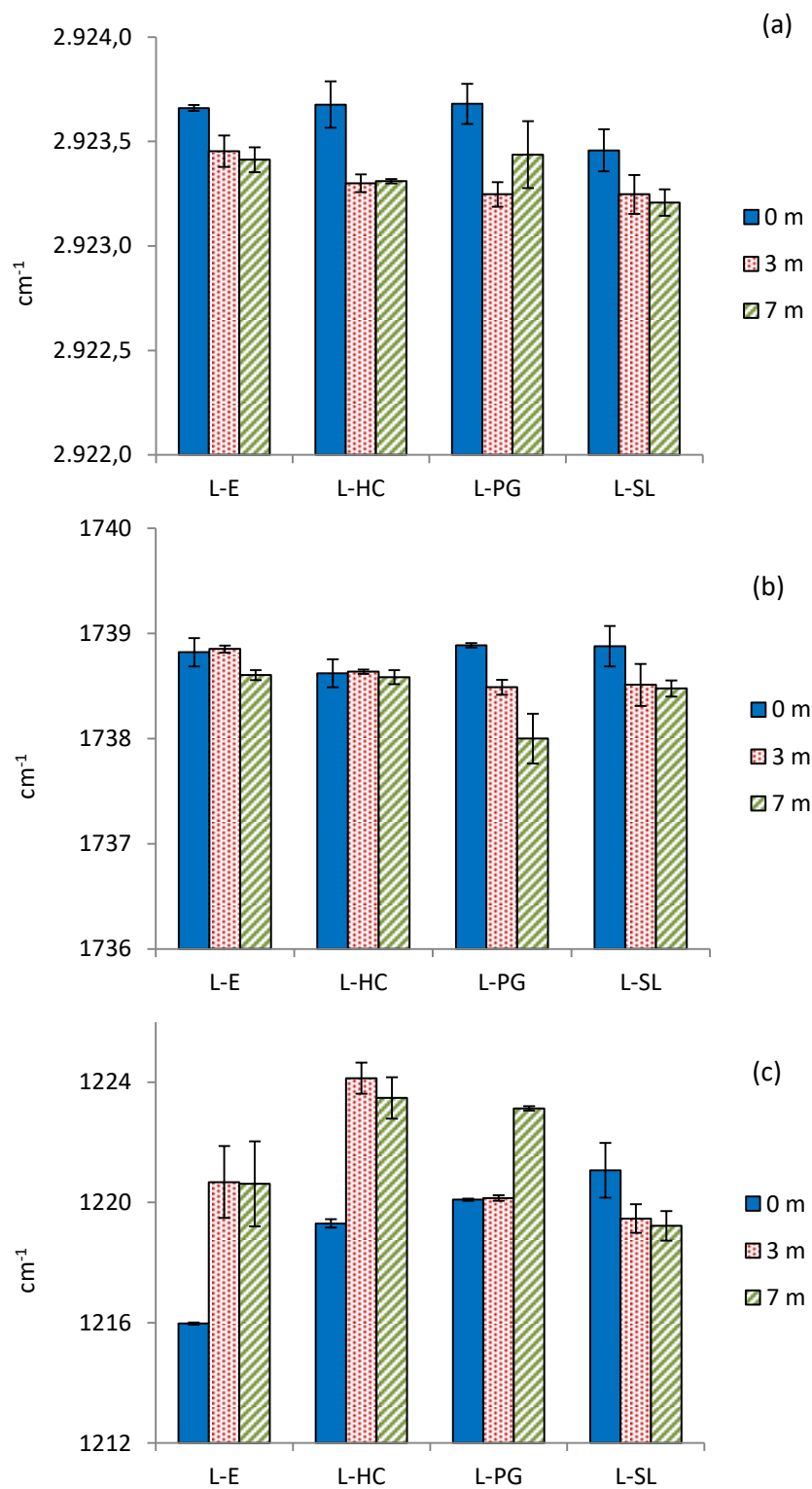


FIGURE 4. Frequency variations in stretching modes of selected functional groups determined in freeze-dried liposomal pastes: (a) CH<sub>2</sub> asymmetric stretching vibration; (b) C=O stretching vibration; (c) PO<sub>2</sub><sup>-</sup> antisymmetric double bond stretching vibration. L-HC: liposomes with collagen hydrolysate; L-PG: liposomes with pomegranate extract; L-SL: liposomes with shrimp lipid extract.

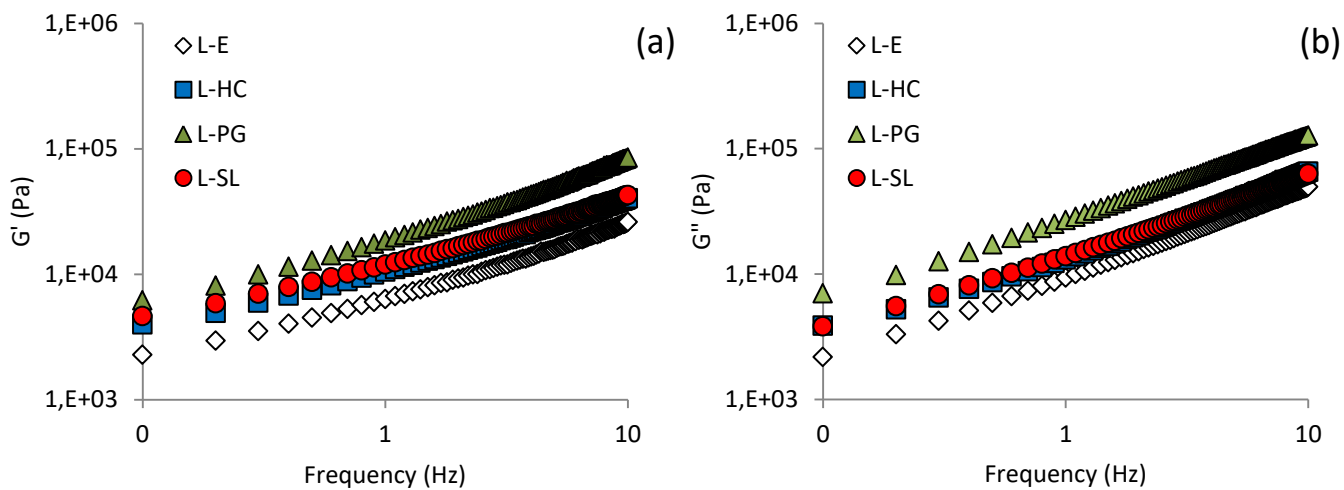


FIGURE 5. Mechanical spectra of newly freeze-dried liposomal pastes: (a) Elastic modulus ( $G'$ , Pa); (b) Viscous modulus ( $G''$ , Pa).

L-HC: liposomes with collagen hydrolysate; L-PG: liposomes with pomegranate extract;  
 L-SL: liposomes with shrimp lipid extract

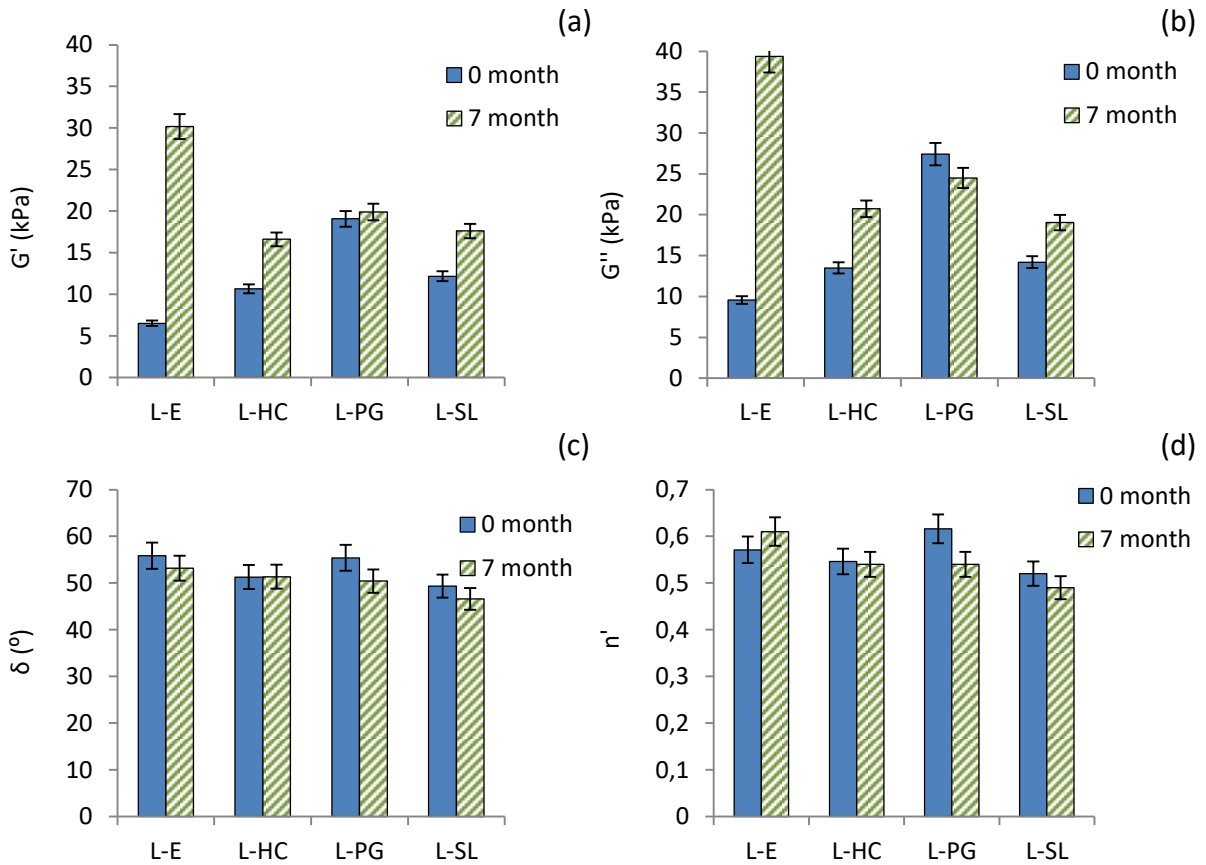


FIGURE 6. Viscoelastic parameters, determined at 1 Hz, of the newly freeze-dried liposomal pastes and pastes stored for 7 months: (a) Elastic modulus ( $G'$ , Pa); (b) Viscous modulus ( $G''$ , Pa); (c) phase angle ( $\delta$ , °); (d) power law exponent ( $n'$ ). L-HC: liposomes with collagen hydrolysate; L-PG: liposomes with pomegranate extract; L-SL: liposomes with shrimp lipid extract.

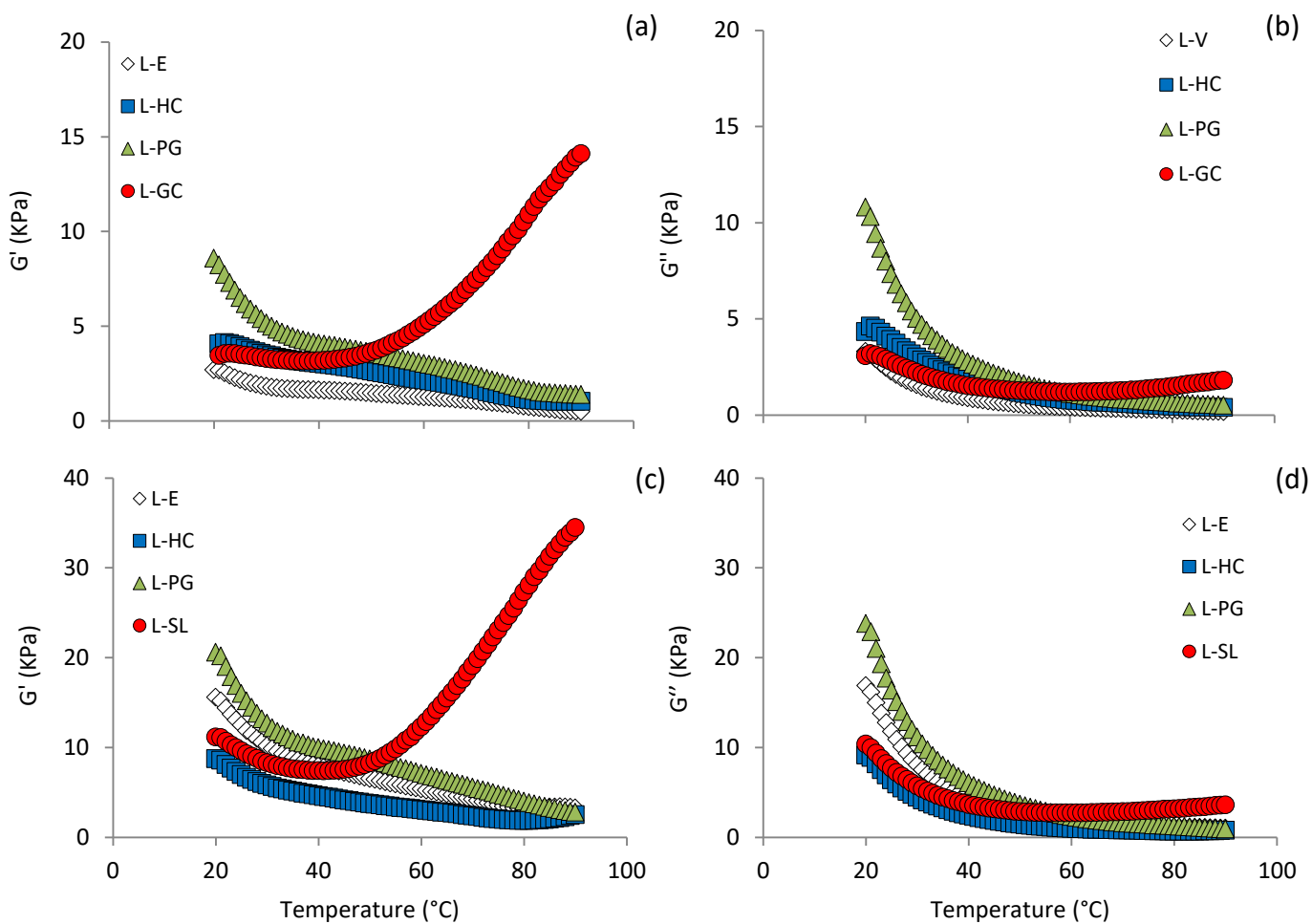


FIGURE 7. Viscoelastic properties as a function of temperature of the newly freeze-dried liposomal pastes : (a) Elastic modulus ( $G'$ , Pa), (b) Viscous modulus ( $G''$ , Pa); and pastes stored for 7 months: (c) Elastic modulus ( $G'$ , Pa), (d) Viscous modulus ( $G''$ , Pa).

L-HC: liposomes with collagen hydrolysate; L-PG: liposomes with pomegranate extract; L-SL: liposomes with shrimp lipid extract.

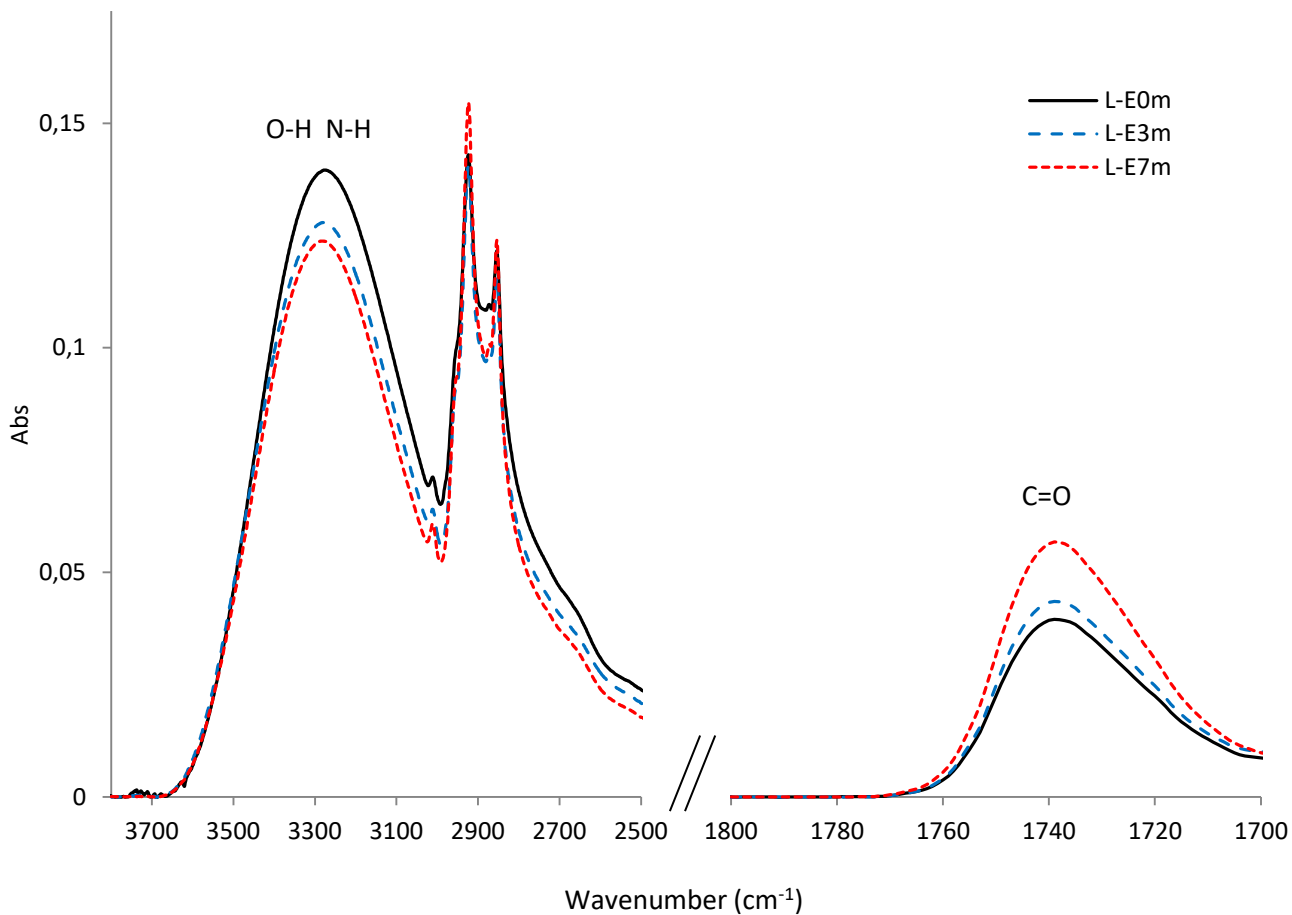


FIGURE 8. Infrared spectroscopy (ATR-FTIR) changes associated to lipid oxidation in freeze-dried empty liposomes (L-E) during seven months of frozen storage .